Determination of humeral inclination in stemless shoulder arthroplasty using plain radiographs

Sascha Beck,1 Robert J. Martin,2 Theodor Patsalis,3 Manuel Burggraf,1 Andrés Busch,3 Stefan Landgraebere,4 Wegner Alexander1

1Department of Orthopaedics and Trauma Surgery, University Hospital Essen, University of Duisburg-Essen, Essen; 2Faculty of Mathematics, University of Duisburg-Essen, Essen; 3Department of Shoulder, Elbow, Hand and Foot Surgery, St. Josef Hospital, Wuppertal; 4Department for Orthopaedics and Trauma Surgery, Saarland University Medical Center and Saarland University Faculty of Medicine, Hamburg, Germany

Abstract

Plain radiographs of the shoulder are routinely used to assess implant orientation after shoulder arthroplasty. Recently, humeral inclination has come into focus especially in reverse stemless shoulder arthroplasty. But, in X-ray projections not exactly parallel to the base of the humeral component, the humeral inclination angle cannot be determined precisely. Therefore, we established a mathematical algorithm to calculate the humeral neck shaft angle and counterchecked the formula using plain radiographs of a sawbone model containing a humeral head prosthesis. With increasing angles of retroversion, the base of the humeral component forms an ellipse in plain radiographs. Knowing the length and width of the ellipse as well as the inclination angle in a plain radiograph, the exact inclination angle can be determined using the equation reported below. Thus, independent from the viewing angle or angle of retroversion, the inclination angle of a stemless humeral head implant can be estimated with an accuracy of ±1.5-degree deviation. The algorithm proposed may be the basis for further research on the impact of humeral inclination in stemless shoulder arthroplasty.

Introduction

In the last decade total shoulder arthroplasty (TSA) has undergone a vast evolution. Meanwhile most companies provide stemless implants for anatomic TSA, several companies even offer stemless implants for reverse shoulder arthroplasty (RSA). Stemless components enable restoration of proximal humeral anatomy independent on humeral shaft orientation. Thus, center of rotation, inclination, retroversion and offset can be reproduced more accurately.1,3 In anatomic TSA, malpositioning of both the humeral and glenoid components adversely affect the range of motion, kinematics, and stability of the shoulder. Therefore, TSA should adapt to the individual’s anatomy and pathology to reconstruct the shoulder to mimic natural anatomy and function.4,5

In RSA humeral inclination can be adjusted as required when using stemless implants. Inclination of the humeral component is of special interest in reverse total shoulder arthroplasty. A high angle of humeral inclination is associated with an increased rate of scapular notching,6 whereas a low humeral neck shaft angle has been found to be associated with an improvement in range of motion in onlay reverse shoulder arthroplasty.7 Plain radiographs of the shoulder are routinely used to assess implant orientation after TSA. In plain radiographs humeral inclination can only be measured accurately if the X-ray beam (viewing angle) is exactly parallel to the retroversion angle of the humeral component. In standard antero-posterior X-ray projections of the shoulder this is rarely the case. When viewing the humeral head component in a non-orthograde manner, the base of an anatomical implant as well as the cup of a reverse humeral implant form an ellipse (Figure 1).

In these projections the base of the humeral component is not parallel to the viewing angle, making it difficult to determine the exact humeral inclination.

The purpose of this paper is to describe a simple and precise method of measuring the humeral inclination angle in standard plain radiographs of the shoulder.

Materials and Methods

Theoretical mathematical deliberations were undertaken for determination of the humeral neck shaft angle (humeral inclination) when looking at a prosthetic humeral head implant at an angle. The angle θ between the orthogonal plane of the head component base (circle) and the viewing direction is given by

\[ \theta = \arccos \left( \frac{b}{a} \right), \]

where \( a \) and \( b \) denote the radii of the minor and major axes of the projected ellipse. An equivalent formula was previously given by McLaren8 for the angle \( \beta \) between the bounding plane of the hemisphere and the viewing axis (Figure 2). Consider an orthogonal coordinate basis \( \{e_x, e_y, e_z\} \) with the unit vectors \( e_x \) and \( e_y \) pointing in distal direction of the humerus and in the viewing direction, with the unit vector \( e_z \) chosen to comply with the right-hand rule. Let \( x \) denote the unit vector in direction orthogonal to the plane of the prosthetic head’s base. Then the inclination is the angle \( \alpha \) between \( x \) and \( e_z \), as visualized in Figure 3.

In terms of corresponding spherical coordinates, the azimuth \( \phi \) of \( x \) is the projected angle between the base of the humeral component and the humerus pointing in distal direction, which is the apparent inclination measured in the radiograph, whereas the polar angle of \( x \) is exactly the angle \( \theta \) between the viewing axis and the joint axis computed in (1). In particular, the first component \( x_z \) of the unit vector \( x \) is given by \( x_z = \sin(\theta) \cos(\phi) \). Since \( x = e_z \), for the dot product between \( x \) and the basis vector \( e_z \),
\[ \cos(\alpha) = \cos\left(\varphi(x, e_1)\right) = x \cdot e_1 = x_1 = \sin(\theta) \cos(\varphi) = \sin\left(\arccos\left(\frac{a}{b}\right)\right) \cos(\varphi) = \sqrt{1 - \left(\frac{a}{b}\right)^2} \cos(\varphi). \]

Thus, the inclination \( \alpha \) is given by

\[ \alpha = \arccos\left(\sqrt{1 - \left(\frac{a}{b}\right)^2} \cdot \cos(\varphi)\right). \]  

If the x-ray beam is perpendicular to the humeral shaft axis, the above formula (2) can be applied to calculate the inclination of a prosthetic humeral component on plain radiographs.

The accuracy of the theoretical calculation of humeral inclination was counterchecked by a radiographic model of the humerus. A sawbone model of a left humerus was used for the radiographic study. The humeral head of the sawbone was resected and a stemless humeral head prosthesis was inserted at the at the anatomical neck (Affinis short, Mathys AG, Bettlach, Switzerland). The sawbone model was installed on a tray using the distal part of the humeral canal for fixation. A wooden peg was positioned onto the distal humerus serving as a pointer for measuring rotation, parallel to the retroversion of the implant (Figure 4). The plane parallel to the humeral cut was determined under fluoroscopic control, when the base of the humeral head implant projected as a line. This position was defined as 0 degrees. Starting at 0 degrees.

### Table 1. Aberration of calculated inclination angle (CIA) using the formula in (3) from real inclination angle (RIA).

<table>
<thead>
<tr>
<th>Retroversion angle</th>
<th>Width of ellipse (a)</th>
<th>Length of ellipse (b)</th>
<th>Measured inclination angle (MIA)</th>
<th>Real inclination angle (RIA)</th>
<th>Calculated Inclination angle (CIA)</th>
<th>Aberration from real inclination angle</th>
</tr>
</thead>
<tbody>
<tr>
<td>0</td>
<td>0</td>
<td>7.94</td>
<td>129.6</td>
<td>129.6</td>
<td>-</td>
<td>-</td>
</tr>
<tr>
<td>5</td>
<td>0.56</td>
<td>7.84</td>
<td>129.7</td>
<td>129.6</td>
<td>129.57</td>
<td>-0.02</td>
</tr>
<tr>
<td>10</td>
<td>1.29</td>
<td>7.34</td>
<td>130.0</td>
<td>129.6</td>
<td>129.35</td>
<td>-0.25</td>
</tr>
<tr>
<td>15</td>
<td>2.12</td>
<td>7.99</td>
<td>130.4</td>
<td>129.6</td>
<td>128.67</td>
<td>-0.93</td>
</tr>
<tr>
<td>20</td>
<td>2.68</td>
<td>7.83</td>
<td>131.0</td>
<td>129.6</td>
<td>128.30</td>
<td>-1.30</td>
</tr>
<tr>
<td>25</td>
<td>3.02</td>
<td>8.00</td>
<td>131.4</td>
<td>129.6</td>
<td>127.76</td>
<td>-1.84</td>
</tr>
<tr>
<td>30</td>
<td>3.49</td>
<td>7.97</td>
<td>133.3</td>
<td>129.6</td>
<td>128.07</td>
<td>-1.53</td>
</tr>
<tr>
<td>35</td>
<td>3.98</td>
<td>7.93</td>
<td>134.7</td>
<td>129.6</td>
<td>127.47</td>
<td>-2.13</td>
</tr>
<tr>
<td>40</td>
<td>4.36</td>
<td>7.95</td>
<td>137.7</td>
<td>129.6</td>
<td>128.21</td>
<td>-1.39</td>
</tr>
<tr>
<td>45</td>
<td>4.68</td>
<td>7.93</td>
<td>139.9</td>
<td>129.6</td>
<td>128.13</td>
<td>-1.47</td>
</tr>
<tr>
<td>50</td>
<td>4.82</td>
<td>7.93</td>
<td>140.2</td>
<td>129.6</td>
<td>127.59</td>
<td>-2.01</td>
</tr>
<tr>
<td>55</td>
<td>5.10</td>
<td>7.83</td>
<td>141.8</td>
<td>129.6</td>
<td>127.00</td>
<td>-2.60</td>
</tr>
<tr>
<td>60</td>
<td>5.28</td>
<td>7.95</td>
<td>145.6</td>
<td>129.6</td>
<td>128.09</td>
<td>-1.51</td>
</tr>
<tr>
<td>65</td>
<td>5.46</td>
<td>7.95</td>
<td>149.3</td>
<td>129.6</td>
<td>128.68</td>
<td>-0.92</td>
</tr>
<tr>
<td>70</td>
<td>5.64</td>
<td>7.57</td>
<td>158.0</td>
<td>129.6</td>
<td>130.30</td>
<td>+0.70</td>
</tr>
</tbody>
</table>

Figure 1. Anteroposterior radiographic views of stemless total shoulder implants. The bases of the humeral components form an ellipse, current humeral inclination, (a) anatomical (b) reverse Total Evolutive Shoulder System (TESS), Biomet, Warsaw, IN, USA.

Figure 2. Two differently oriented circles with radius b, observed from different directions.

---

[Orthopedic Reviews 2019; 11:8194]
degrees, x-rays of the sawbone model were taken with increasing angles of retroversion. An x-ray was taken every 5 degrees between 0 and 70 degrees of retroversion.

Results

At 0 degrees of retroversion the ‘real inclination angle’ (RIA) of the sawbone model measured 129.6 degrees. With increasing angle of retroversion, the base of the humeral head prosthesis projected as an ellipse on plain radiographs (Figure 4). The ellipse with its two axes was delineated in each x-ray projection. Humeral inclination was measured using one axis perpendicular to the base of the ellipse and the other axis parallel to the humeral shaft. The angle formed between the two axes was named ‘measured inclination angle’ (MIA). With increasing angles of retroversion, the ellipse gained in width, whereas the length did not significantly change. With higher angles of retroversion, the MIA was found to increase up to 158.0 degrees at 70 degrees of retroversion (Table 1).

Knowing the width \(a\) and \(b\), length of the projected ellipse as well as the MIA (\(\varphi\)), the RIA could be calculated using the following formula:

\[
\text{arccos} \left( \frac{a^2}{b^2} \cdot \cos(\varphi) \right). \quad (3)
\]

Discussion

Plain radiographs of the shoulder are routinely used to assess implant positioning in total shoulder arthroplasty, but measuring humeral inclination may be inaccurate due to projectional error. This poses a real challenge when stemless humeral implants are used, which enable placement of the humeral component independent from the humeral shaft axis. In contrast to stemmed humeral implants the surgeon is now free to choose inclination of the humeral implant.1,9-14 The described method for measuring anteversion of an acetabular cup from standard anteroposterior radiographs15-17 could not be easily transferred to the shoulder, since the base of the humeral component forming an ellipse is affected in two planes when the humeral head is rotated.

In our study, we demonstrate that the measured humeral inclination angle depends on the viewing- and retroversion angle of the implant on x-rays and the estimated value erroneously increases with advancing retroversion angle. We observed, that the apparent humeral inclination, as measured on plain radiographs, corresponds to the true humeral inclination when humeral retroversion does not exceed 25 degrees. Humeral inclination only increased from 129.6 degrees in neutral rotation to 131.4 degrees at 25 degrees of retroversion.
Variability amounted to less than 2 degrees and could also be due to inaccuracy when measuring humeral inclination. However, for exact determination of humeral inclination on plain radiographs, an algorithm is required which generates the real inclination angle (RIA) independent of the viewing angle/retroversion angle. With varying angles, the base of the humeral component forms an ellipse with two axes. Knowing the minor and major axes of the ellipse as well as measuring humeral inclination (MIA), the real inclination angle (RIA) can be calculated accurately. In our sawbone model the calculated inclination angle (CIA) varied between 127.00 and 130.30 degrees. Thus, the maximum aberration of the CIA from the RIA was 2.6 degrees. This variation can be attributed to inaccuracy when determining the axes of the ellipse and the MIA. With the formula given (3) the mean deviation of the CIA was less than 1.5 degrees (1.32±0.71 degrees).

Our algorithm was counterchecked using an anatomical humeral head prosthesis. The basis for calculating the real inclination angle consists of measuring the apparent humeral inclination and the axes of the ellipse in plain radiographs. These principles do not only apply to anatomical humeral head components, but also for reverse implants since the base of a reverse humeral head prosthesis also forms an ellipse with increasing angles of retroversion (Figure 1). Thus, using the algorithm introduced, the inclination angle of the humeral component in anatomical and reverse shoulder arthroplasty can be determined precisely.

Our algorithm may be the basis for further research on the effect of humeral inclination in stemless shoulder arthroplasty.

Limitations

We are aware that it is not possible to distinguish retroversion from anteverision of the humeral head prosthesis in plain radiographs. Nevertheless, assuming correct patient positioning and x-ray projection as well as correct implant positioning anteverision is very unlikely since anatomical studies showed that humeral head retroversion averages around 30 degrees.18,19 Furthermore, differentiation of retroversion vs. anteverision has no adverse effect on the calculated inclination angle.

Conclusions

The mathematical algorithm introduced (3) can serve as an important tool for precise determination of humeral inclination in stemless shoulder arthroplasty. Independent from the viewing angle or angle of retroversion the humeral neck shaft angle can be calculated ±1.5-degree deviation.

References